

CONTRIBUTION
OF
NANOTECHNOLOGY
TO
MOLECULAR IMAGING

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Imaging and nanotechnology

We shall focus our purpose on molecular imaging and will conventionally consider two separated access to the molecular level :

the direct one that uses endogenous biophysical process or specific ligands for image contrast formation ;

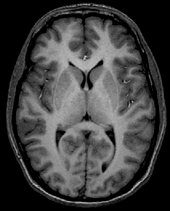
the indirect one that uses nanotechnology to conceptualize engineered **marked probes** so as to visualize cells events at the molecular level.

The marker is an infrared, luminescent or fluorescent probe in optical imaging, a radioactive tracer in TEP or TEMP imaging and a (super)para- or ferro- magnetic contrast agent in MRI.

Let's considering the
direct way to reach the
molecular level:

image formation via
endogenous biophysical
processes and specific probes

T1 & T2 modulations in MRI



... due to physiology or pathology



Positive contrast in $T1_w$ images, negative in $T2_w$

Mobile structures
Liquids (CSF)
 $T_1 = T_2 (\approx 4 \text{ s for H}_2\text{O})$

T_1
 T_2

hours

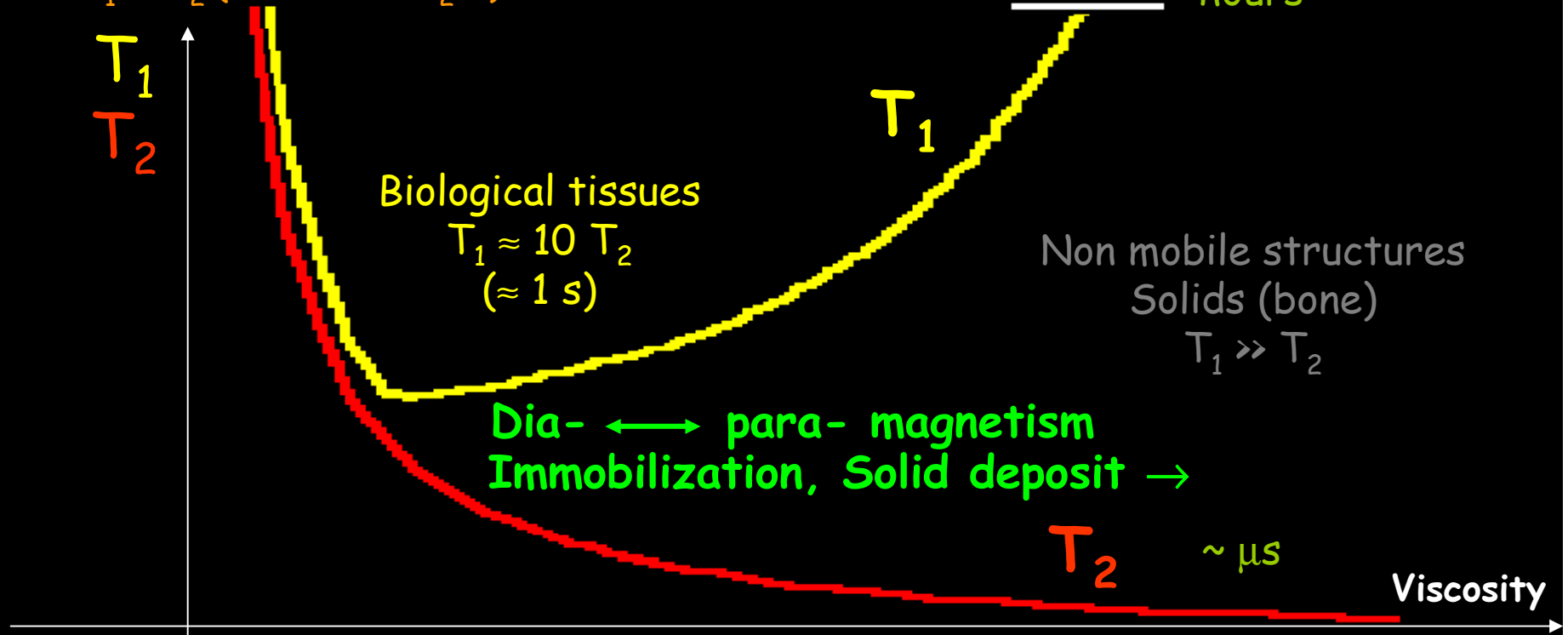
Biological tissues
 $T_1 \approx 10 T_2$
($\approx 1 \text{ s}$)

Non mobile structures
Solids (bone)
 $T_1 \gg T_2$

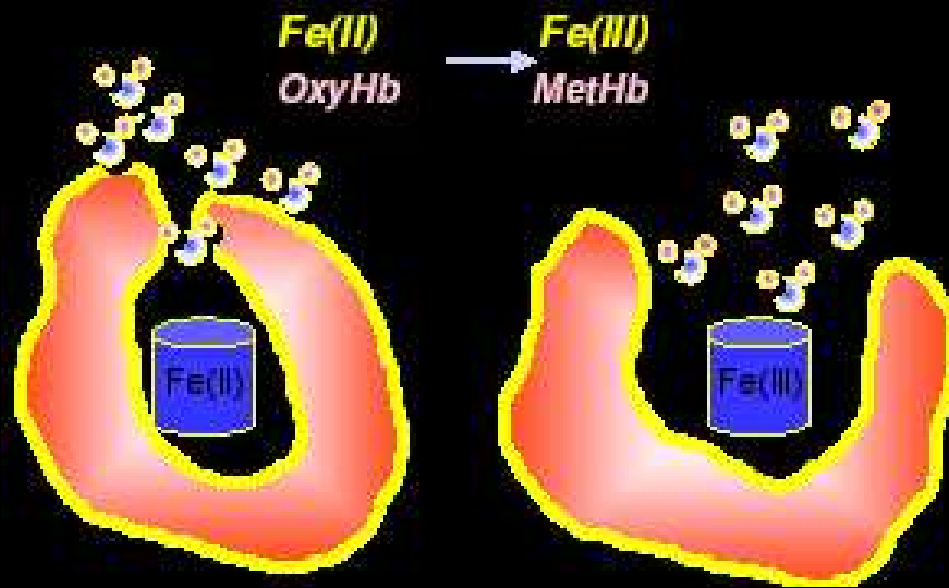
Dia- \longleftrightarrow para- magnetism
Immobilization, Solid deposit \rightarrow

$T_2 \sim \mu\text{s}$

Viscosity



Spontaneous MRI T2* contrast when MetHb replaces HbO₂



HbO₂ is diamagnetic
MetHb is paramagnetic



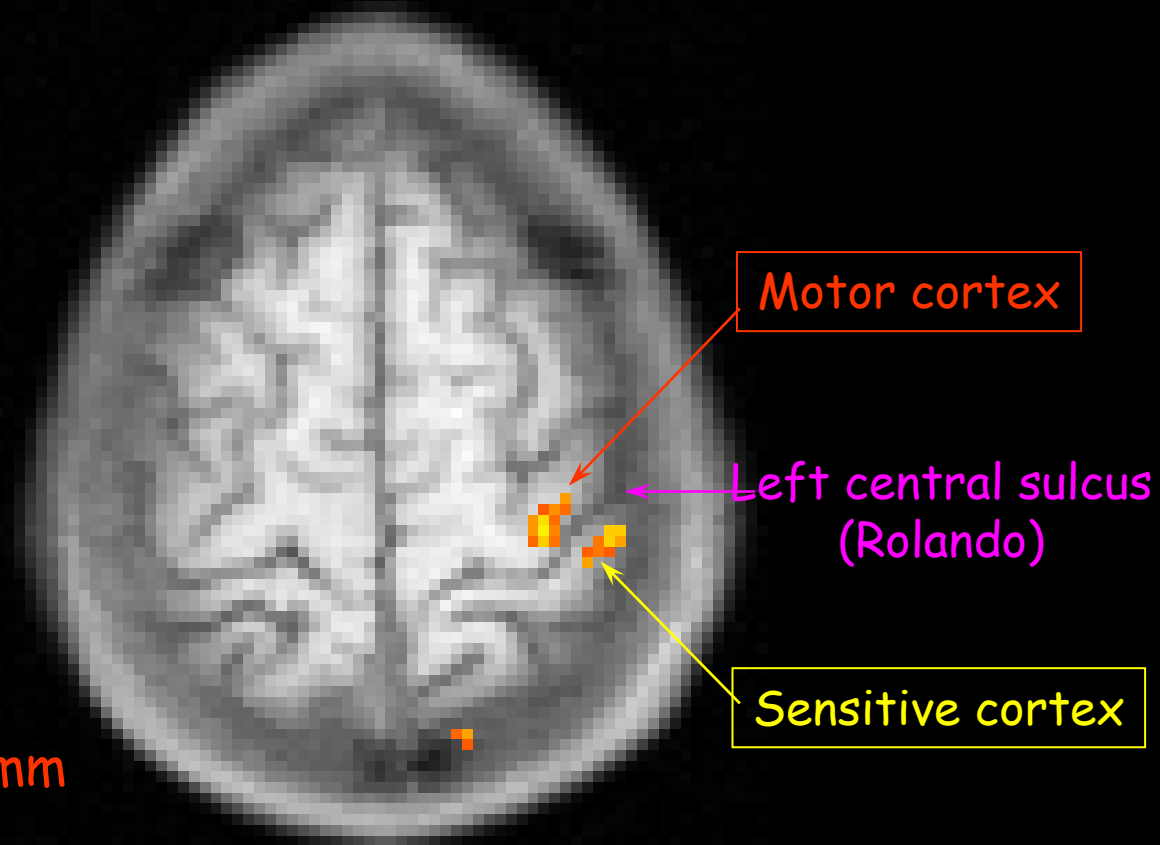
Late aspect of an hemorrhagic stroke

Spontaneous MRI contrast due to an excess of HbO₂ relatively to Hb

HbO₂ is diamagnetic
Hb is paramagnetic

Right handed
subject, pre- and
post- central left
activations

AC-PC + 70 mm

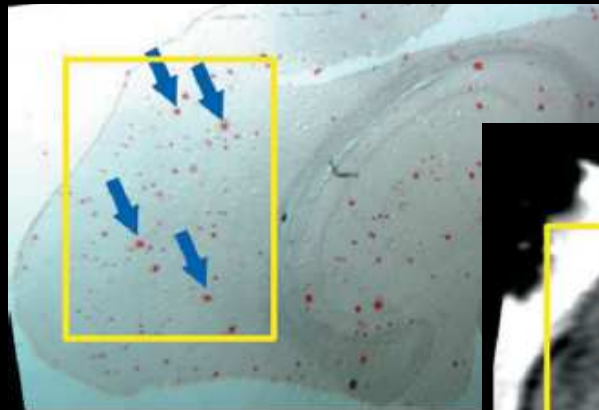


Tactile opposition, right thumb / Vth meta origin

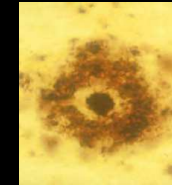
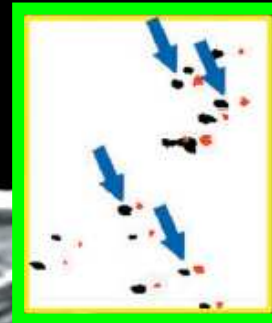
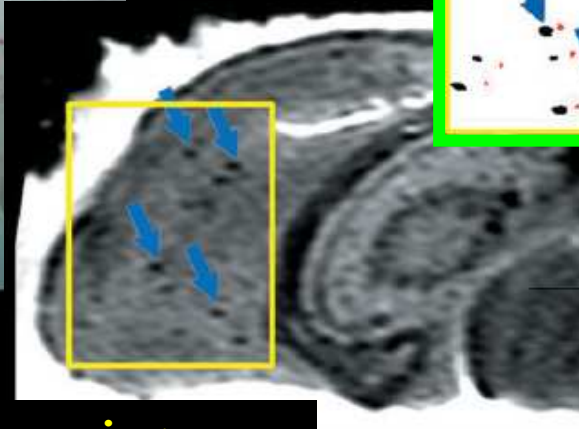
Spontaneous MRI signal loss in solid structures

Ex vivo detection of β amyloidal deposits (Alzheimer)
in $T2_w$ MRI

Histology with Congo red

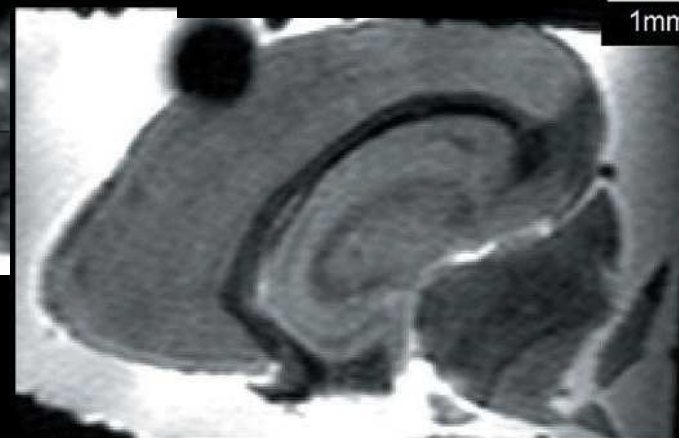


$T2^*$ -MRI



Extra cellular β amyloidal peptides deposits (20-150 μm)
have very short $T2^*$

Control mouse



mAPP-PS1 transgenic mouse

mAPP : mutant human amyloid precursor protein
PS1 : mutant presenilin-1 transgenes

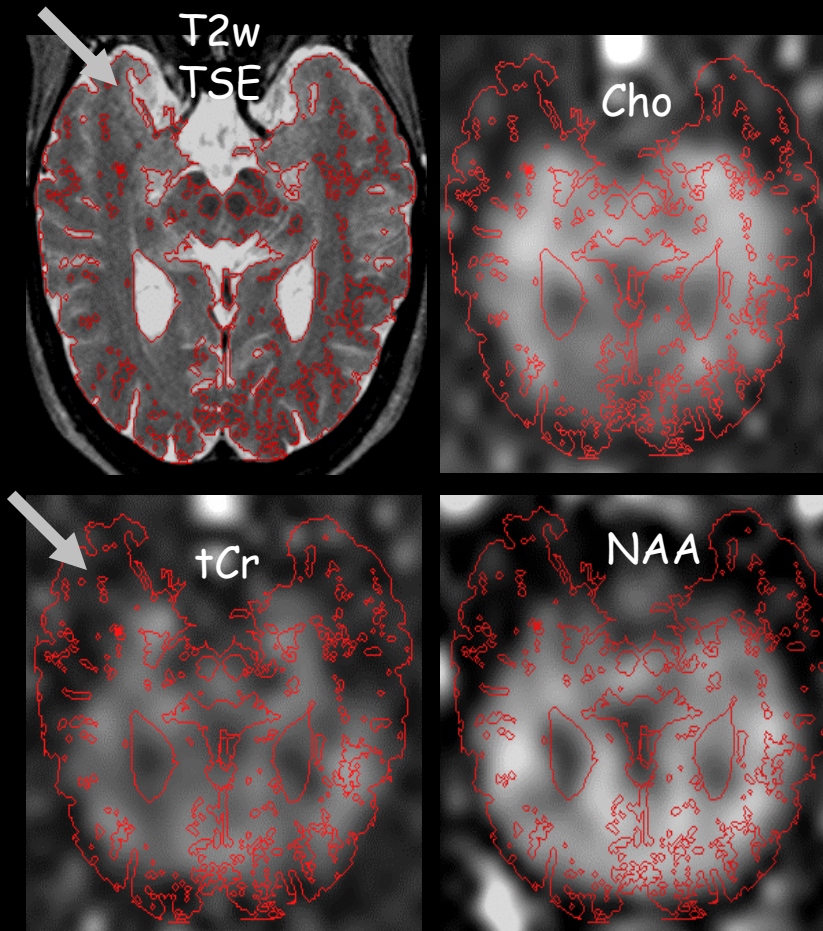
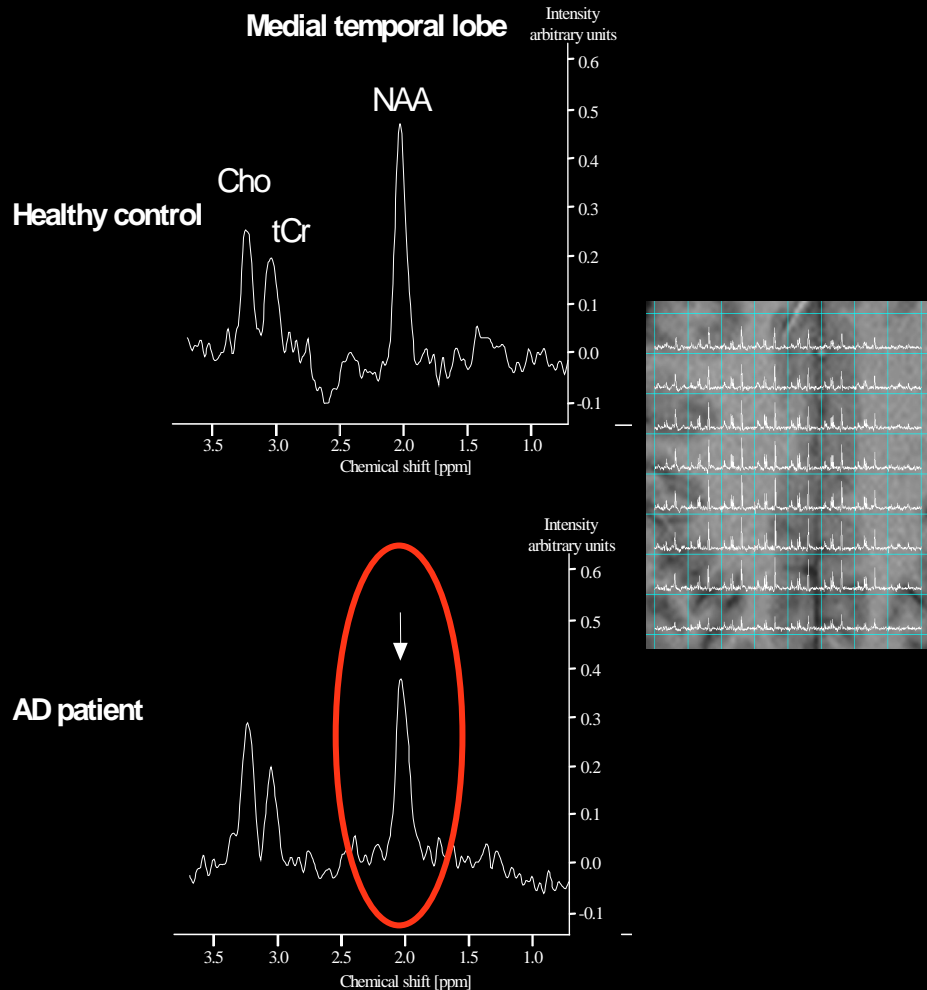
In the **green** surrounded frame, large MRI black spots correspond to amyloidal deposits seen by histology (red dots), moved forward for clarity and to avoid superimposition

Metabolite cartography by ^1H -MRS & CSI

Example of Alzheimer Disease (AD)

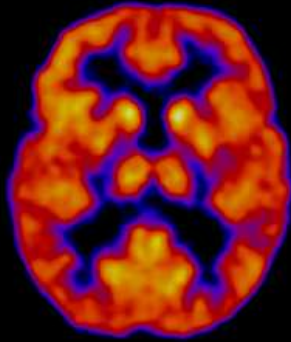
MRS

CSI



Courtesy Gwénaél HÉRIGAULT, Philips Medical Systems, 2002

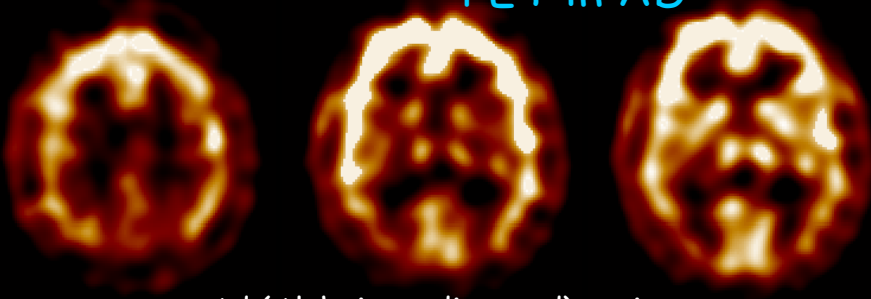
Spontaneous cerebral metabolism of ^{18}F FDG



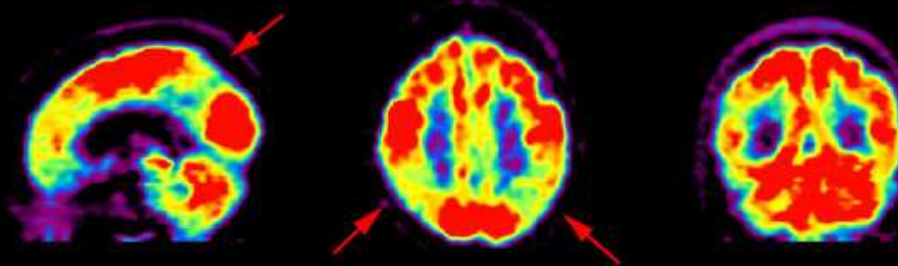
Normal ^{18}F -FDG
TEP image

Glucose metabolism is equivalently distributed in the cortex for a normal (non pathological) brain, but is greatly lowered in specific regions in AD

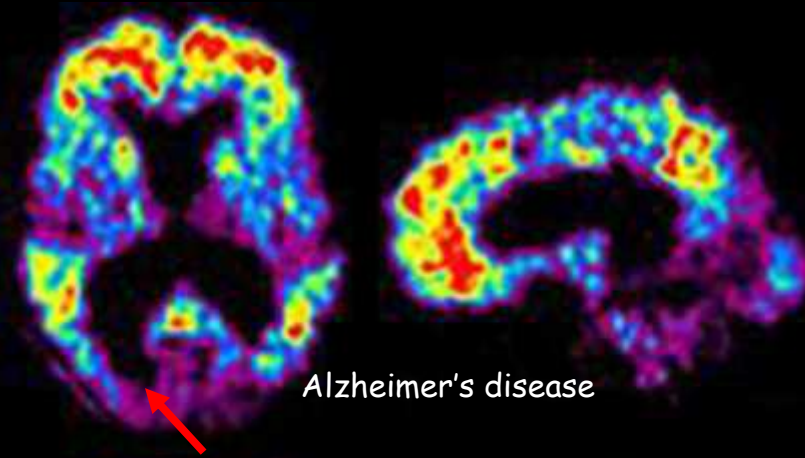
PET in AD



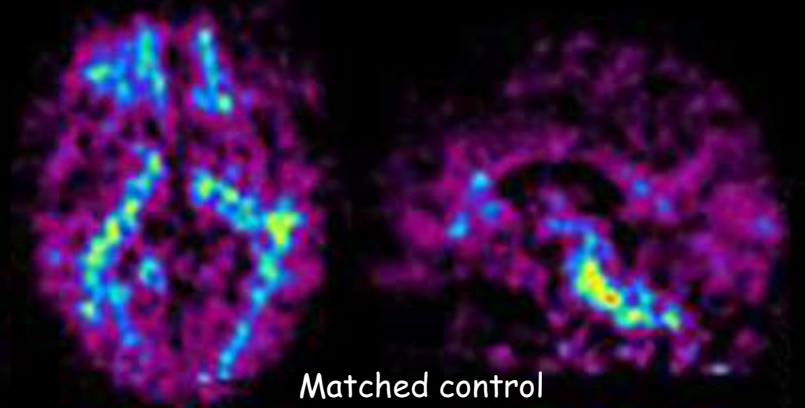
Ad (Alzheimer diseased) patient



Visualizing AD β -amyloids deposits with ^{11}C -PIB PET



Alzheimer's disease



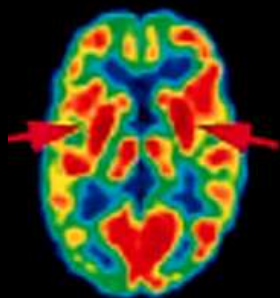
Matched control

KLUNK W, MATHIS C, et al., Pittsburgh, Associated Press posting 12 Jan 2003

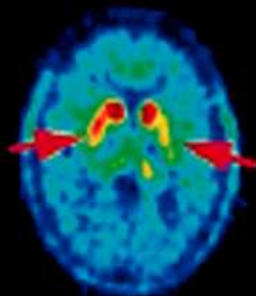
Crude and grafted Parkinson disease



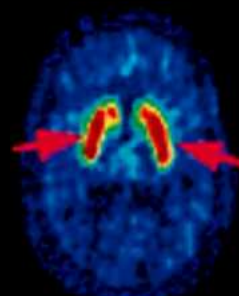
MRI
 ^1H



Metabolism
 ^{18}F FDG



^{18}F -DOPA
Pre-synaptic
DaT



^{18}F -Ethyl
Spiperone
Post-synaptic
 D_2R

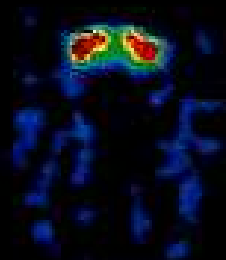
Clinically left
Parkinson

Loss of DaT
function in the right
putamen

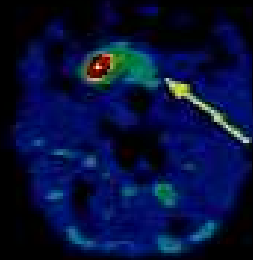
D_2R is normal or a
little higher
(up regulation)

M.E. PHELPS, JNM, 2000 ; 41 : 661-681

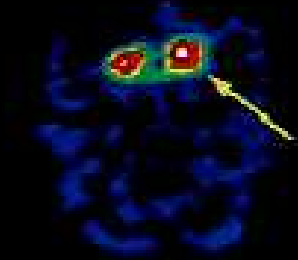
meta- ^{18}F -tyrosine



Normal



Before
Gene Therapy



After
Gene Therapy

Left Parkinson
generated in a
monkey

A Macaques Rhesus
after homolateral
MPTP injection and
grafted stem cells

K. BAUKIEWICZ, in M.E. PHELPS, PNAS, 2000 ; 97(16) : 9226-33

Let's now consider
the indirect way
to reach the
molecular level

using specific "engineered"
probes and ligands to
reveal cells activity

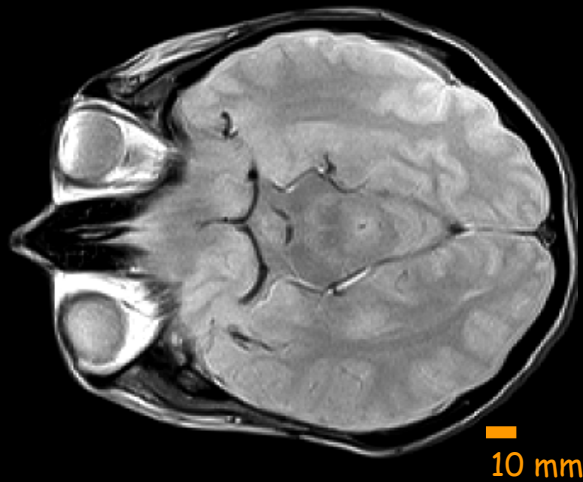
The indirect way to reach the molecular level

Apart a few examples in PET and optical imaging, we'll essentially consider MRI, due to its (very) high spatial resolution and a great variety of possible contrasts

But MRI fails by a (very) low sensitivity and we'll present some examples about how very sophisticated engineered (nano)-techniques will improve it, among which :

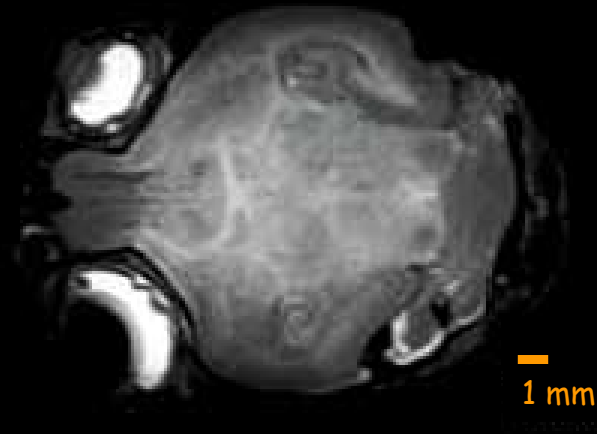
- Development of high relaxivity contrast media
- Amplification of relaxivity and targeting
- Development of smart agents whose action is limited to the targeted site and/or a chosen cellular activity

MRI gives access to the (very) high intrinsic spatial resolution



Healthy human

$$R_{sp}^{\circ} \sim 1 \times 1 \times 1 \text{ mm}^3$$



Mouse tumour

$$R_{sp}^{\circ} \sim 110 \times 110 \times 110 \text{ } \mu\text{m}^3$$



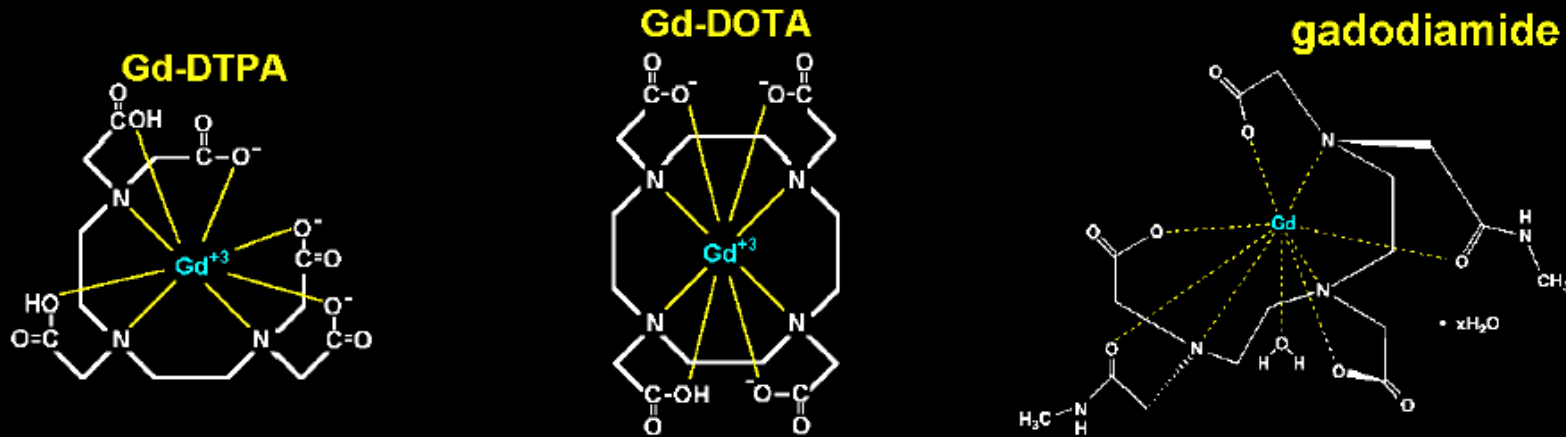
Xenopus larvae

MRI spatial resolution (R_{sp}°) is only limited, for a given contrast, by translational movements of water molecules, of about 2 to 20 μm .

Indirect imaging:
contrast media and probes

MRI paramagnetic contrast media

Gd chelates (hypersignal in T_{1w} MRI, toxics)



High detection threshold, added to the very low MRI sensitivity, implies high concentrations and/or smart amplification techniques

They often are coated and targeted by coupling or conjugation :

- toward receptors,
- toward cells (Gd-EOB-DTPA and hepatocytes)
- toward plaques or clots (conjugation to anti-fibrin antibodies)

MRI superparamagnetic contrast agents

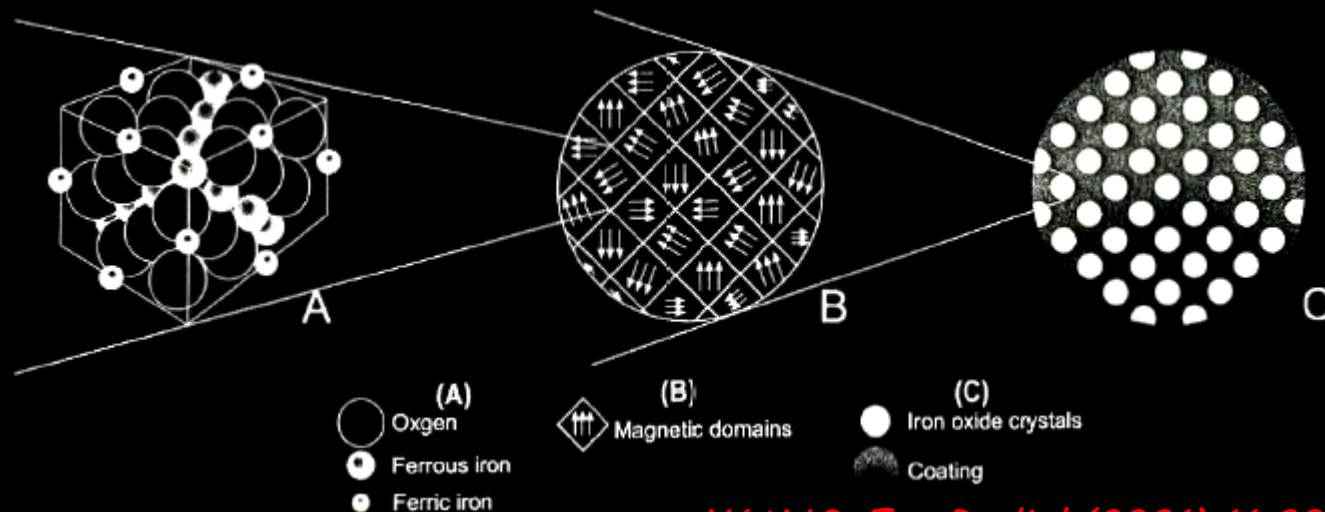
SPIO = Superparamagnetic Iron Oxide ($\varnothing > 50$ nm), marked accumulation in RES (liver, spleen, lymph nodes).

USPIO = Ultrasmall Superparamagnetic Iron Oxide ($\varnothing \sim 10$ -50 nm), far more efficient, with a marked accumulation in monocytes and macrophages (graft reject, plaques of atherosclerosis).

Both SPIO & USPIO have a T2* main effect (hyposignal), with a detection threshold in mM for SPIO, μ M or even nM for USPIO)

MIONs (Monocrystalline Iron Oxide Nanoparticles) are (U)SPIO nanoparticles ($\varnothing \sim 3$ nm with > 2000 Fe atoms) without any molecular specificity.

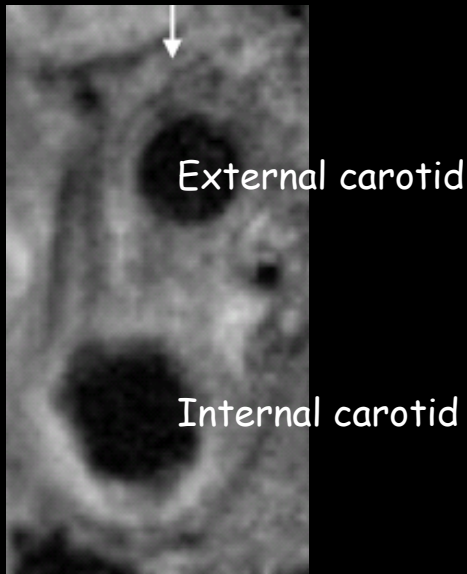
ferrous core
(≤ 5 nm for
USPIO)



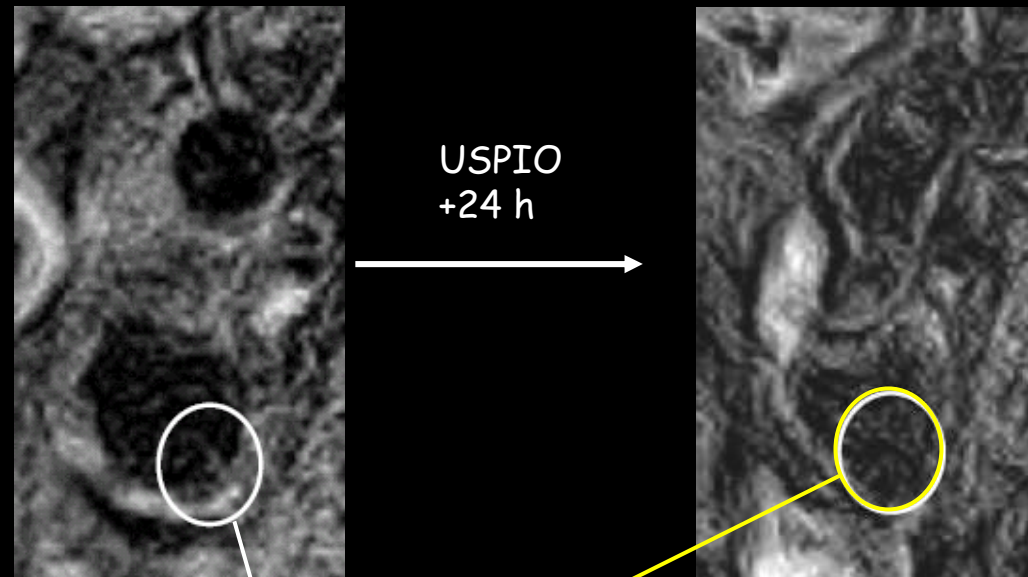
Indirect imaging via passive
probe uptake and elimination

USPIO passive uptake by macrophages allows atherosclerotic plaques detection

MRI



$T2_w^*$ MR images

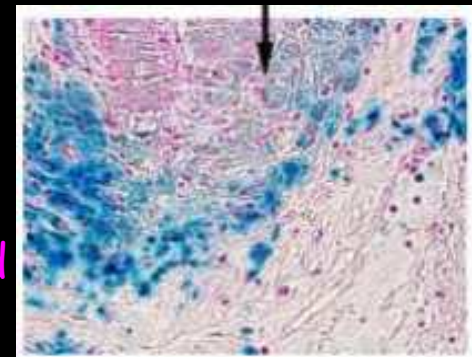


Plaque $T2^*$ hypersignal before contrast

Plaque $T2^*$ hyposignal after USPIO

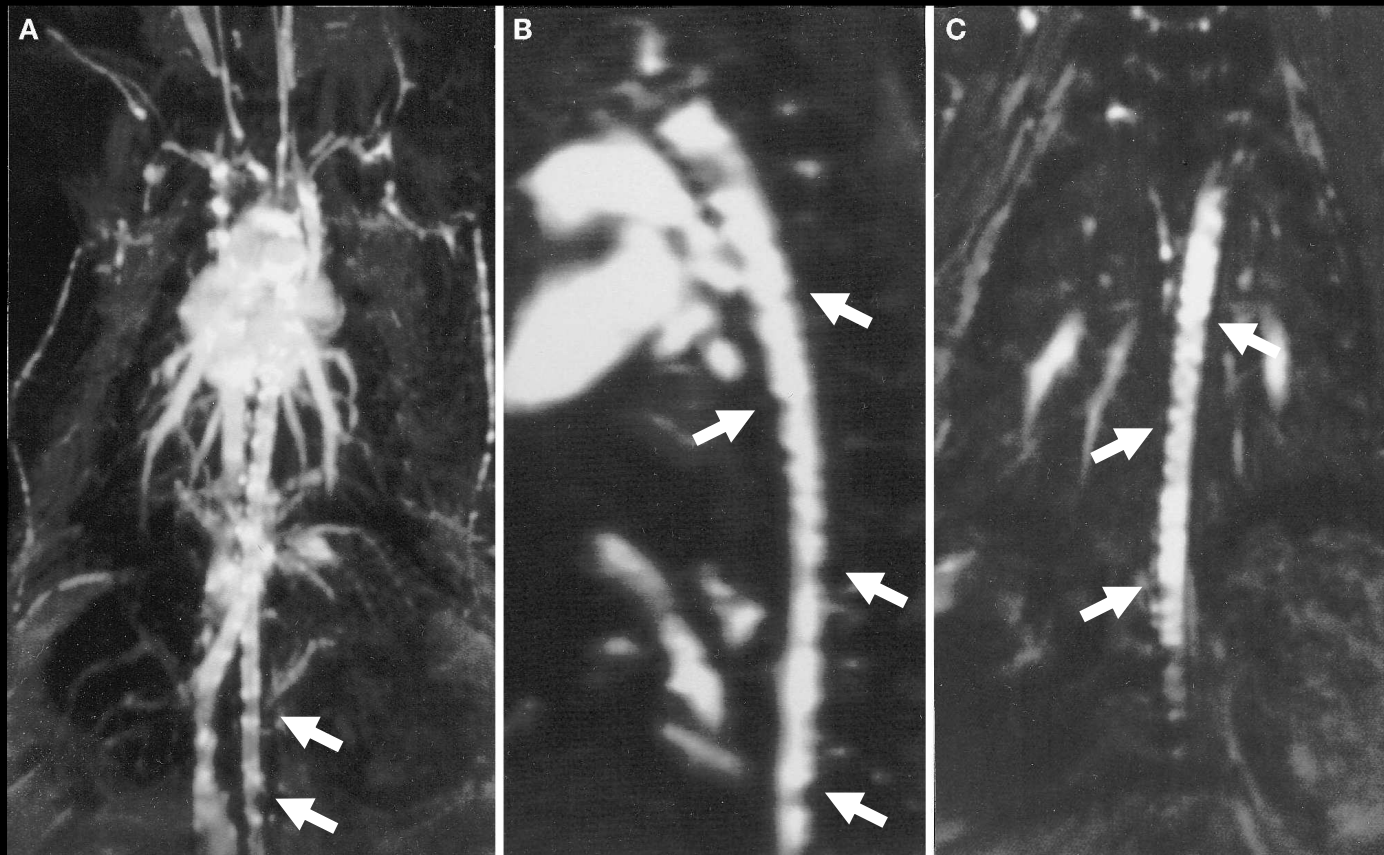
Plaques vulnerability is determined by their macrophages content

Histology :
CD68 (macrophages) - red
Perls (USPIO) - blue



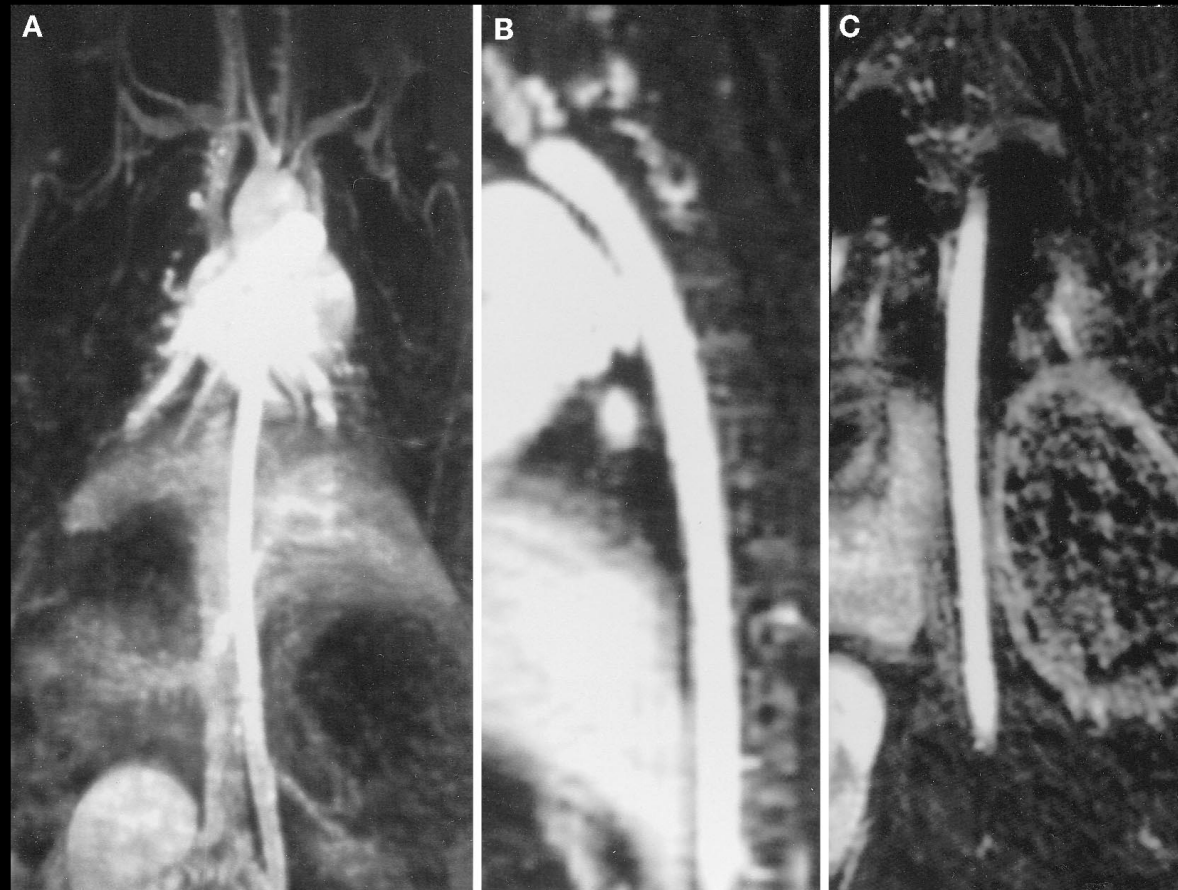
USPIO & vascular plaques detection

7 month old rabbit with hyperlipidemia and atherosclerosis



Hypo signals due to passive Fe uptake in macrophages confined in atherosclerotic plaques

... while, with Gd-DTPA, atherosclerotic plaques are not visible



The same hyperlipidemic rabbit

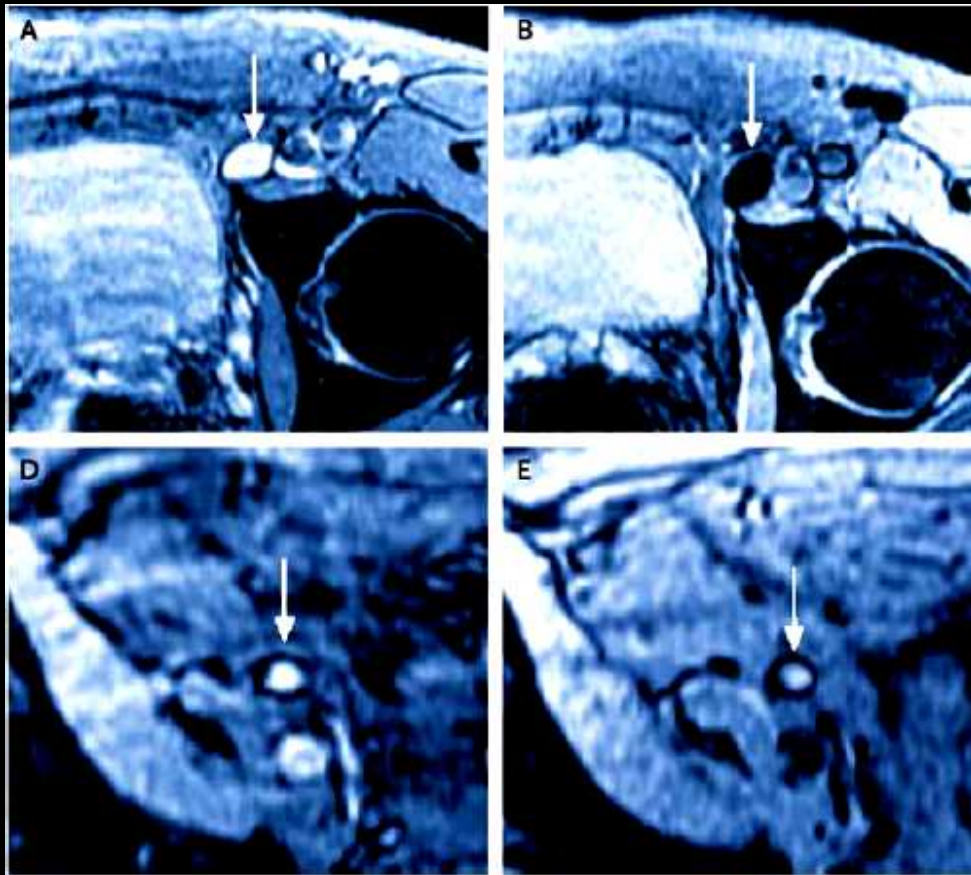
RUEHM, SG et al, Circulation, 2001; 103: 415

USPIO uptake by metastatic lymph nodes

USPIO ($\varnothing \sim 50$ nm) improve diagnosis of metastatic axillary lymph nodes compared with precontrast MRI

before USPIO

after USPIO



Healthy lymph node captures the SPIO
T2* signal is homogeneously decreased

Tumorous lymph node does no more capture the SPIO
Persistent hypersignal

Indirect imaging via targeted probe uptake and elimination

- Targeting at the tissue level
- Targeting at the cellular level
- Targeting at the molecular level

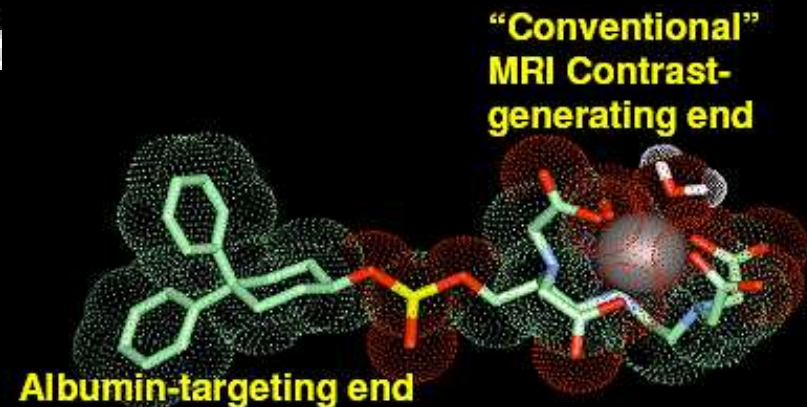
Targeting blood in vessels: Gd Complex coupled to Serum-Albumin

Albumin-binding (MS-325)

Enhanced relaxivity while in the blood
Long life = hi-res blood pool MRA
Phase III on-going



MRI

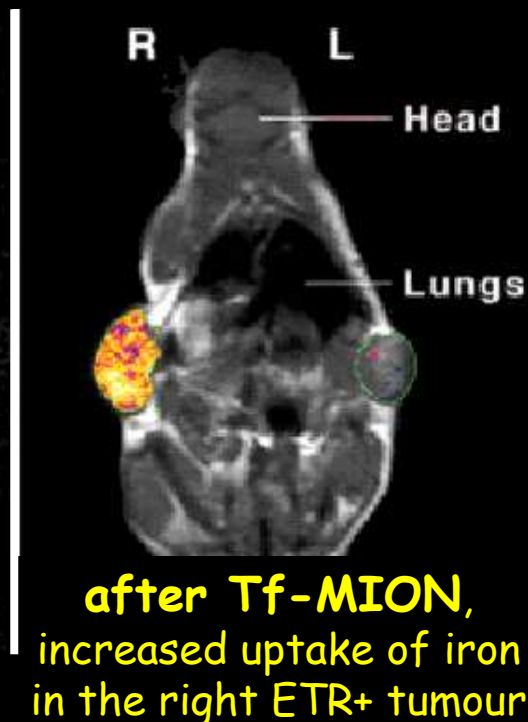
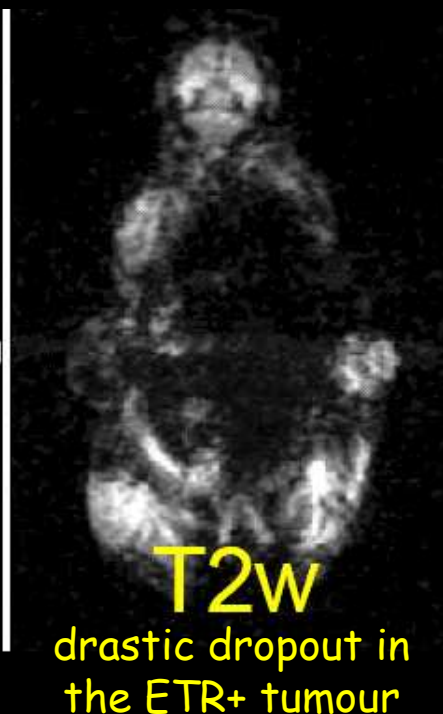
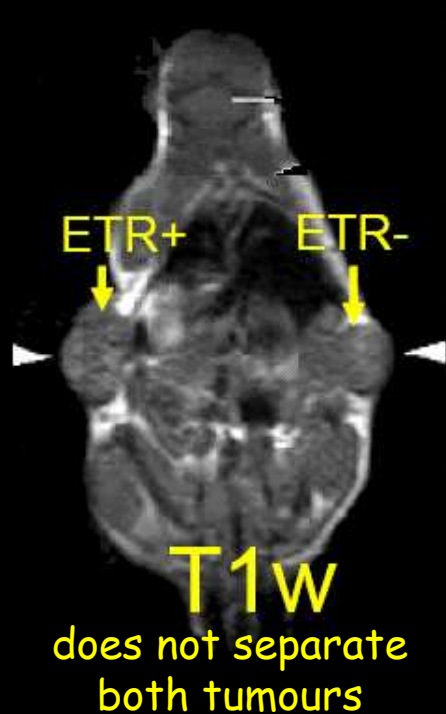


Iliac and femoral vasculature
Richard Baum, M.D.
University of Pennsylvania

From M. MOSELEY, MR role in Molecular Imaging ?, MR4MI_2006

Targeting sarcoma cells with MRI Tf-MION via transferrin receptor overexpression

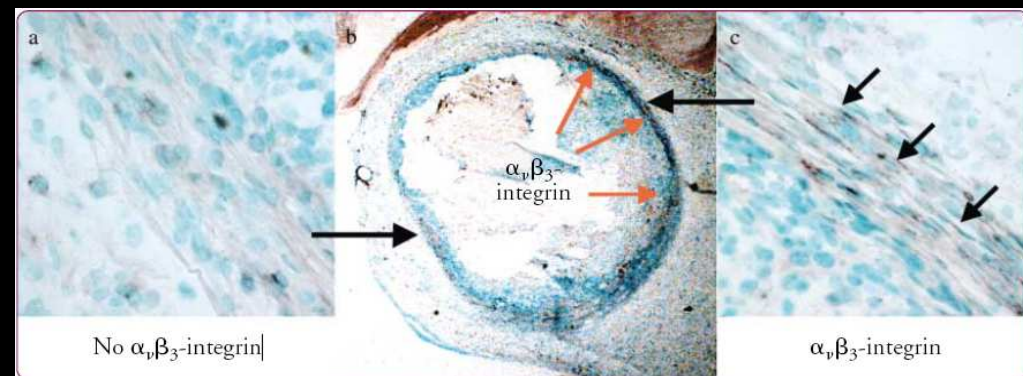
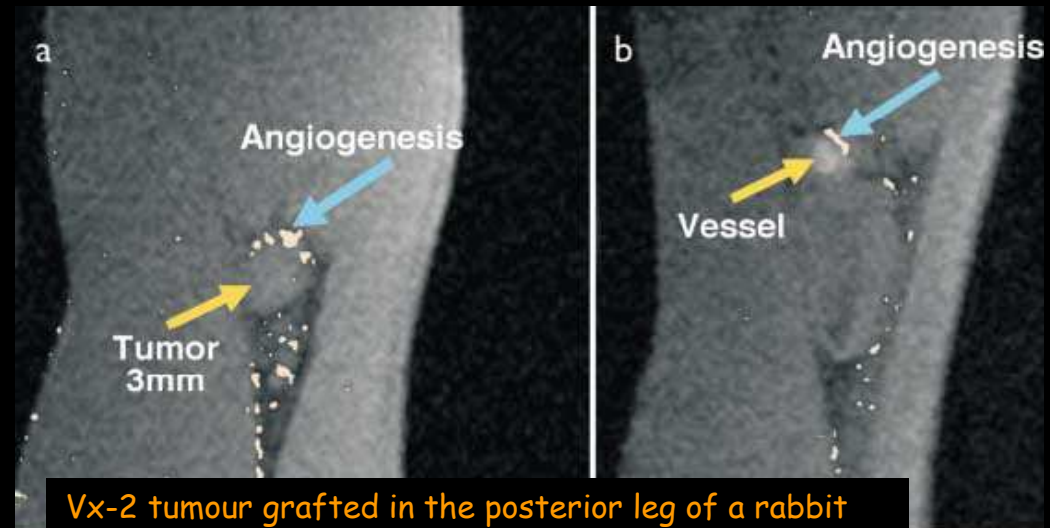
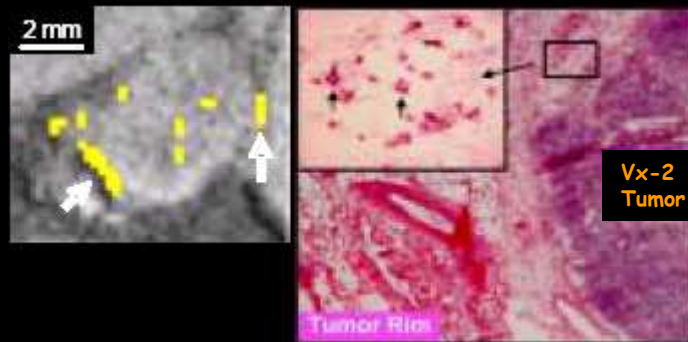
Gliosarcoma cells are stably transfected with an expression plasmid containing engineered transferrin receptor (ETR+) cDNA that overexpresses high levels of the transferrin receptor protein. This will result in a marked increase in the cellular binding and uptake of MION to holotransferrin (Tf-MION), as can be seen in that living mouse with a right ETR+ flank tumour and a left ETR- flank tumour.



Nano particles targeted for endothelial $\alpha_v\beta_3$ -integrin and angiogenesis

Integrin is a membrane receptor that binds peptides as fibronectin and laminin implied in cellular adhesion.

Integrin increases in cancer angiogenesis, at capillaries epithelial cells membranes level

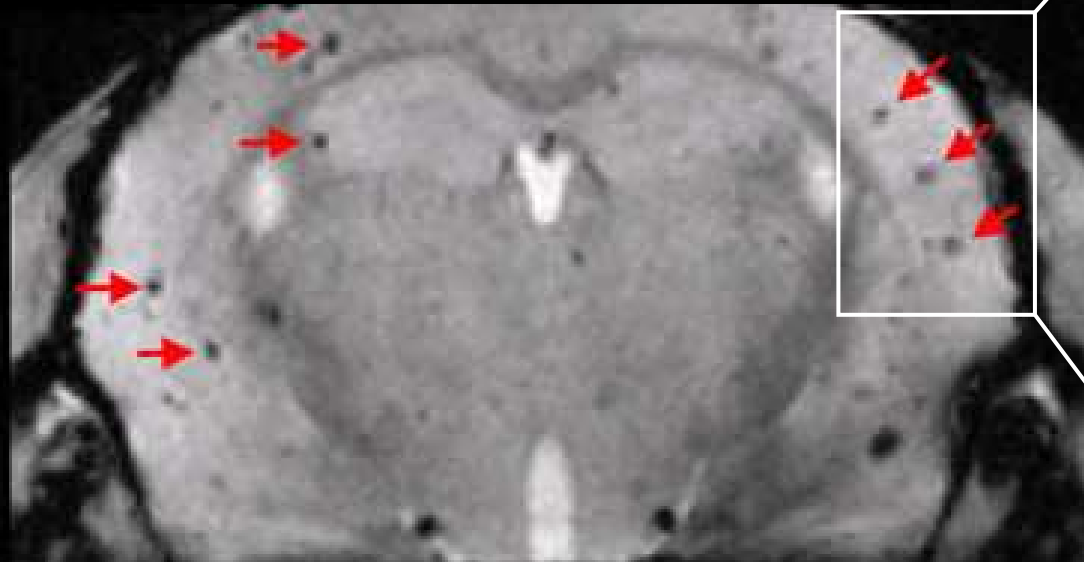


Exact correspondence between histology and MRI

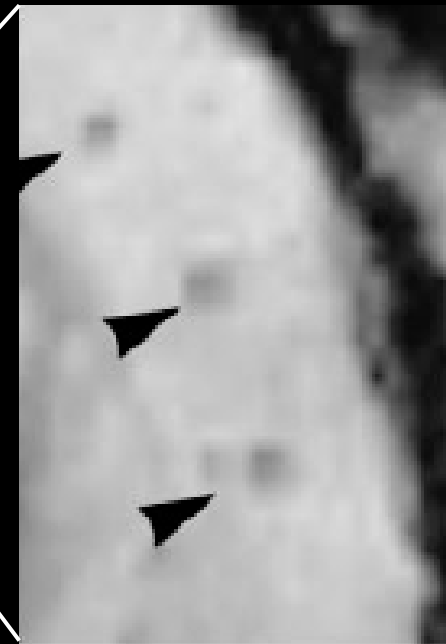
SPIO-peptides targeted for Amyloid β plaques

Magnetically labeled peptides enable in vivo detection of amyloid- β (arrows) in the brains of transgenic mice used to model Alzheimer's Disease

Plaques in *in vivo* T2* MRI
78x78x250 mm, acquisition 59 min



6-month-old APP/PS1-transgenic mouse brain

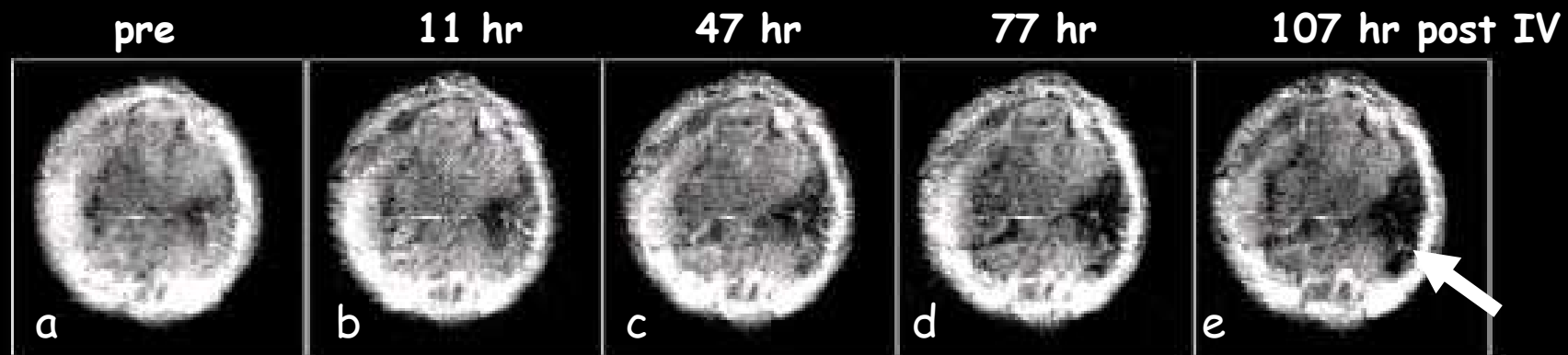


Arrows emphasize the neat agreement with plaques shown by histologic coloration

C2-Synaptotagmin SPIO and apoptosis

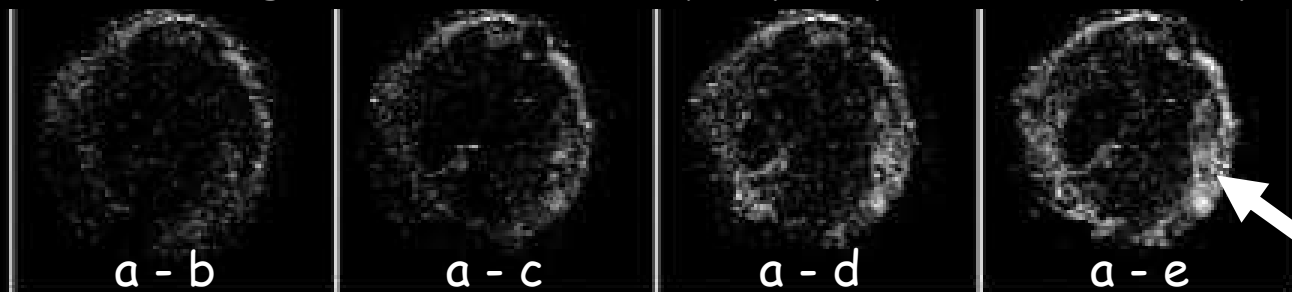
Synaptotagmin I binds to anionic phospholipids (phosphatidylserin, PS). During apoptosis, PS translocates from inner to outer layer of cellular plasma membranes.

Thus, when cells are dying by apoptosis, SPIO conjugated to C2 domain of synaptotagmin I will bind to PS and reveal the apoptotic area (arrow).



Murine lymphoma following treatment with cyclophosphamide and etoposide

Cells in
apoptosis

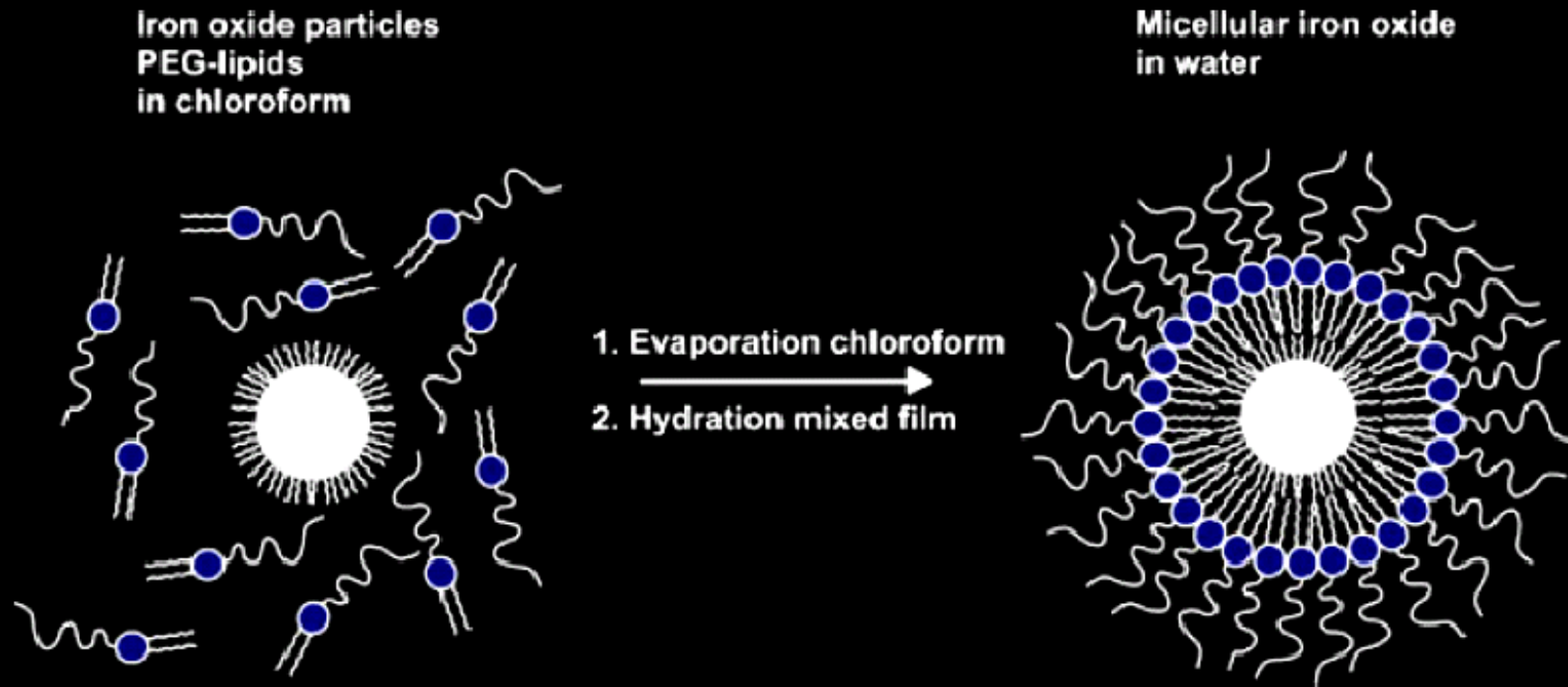


Indirect imaging via contrast over concentration (amplification)

- using (targeted) micelles
- using (targeted) dendrimers
- using carbon nanotubes
- using cellular enrichment in iron affine structures

Nanoparticle-containing micelles

Schematic representation of the encapsulating procedure of hydrophobic nanoparticles in micelles.

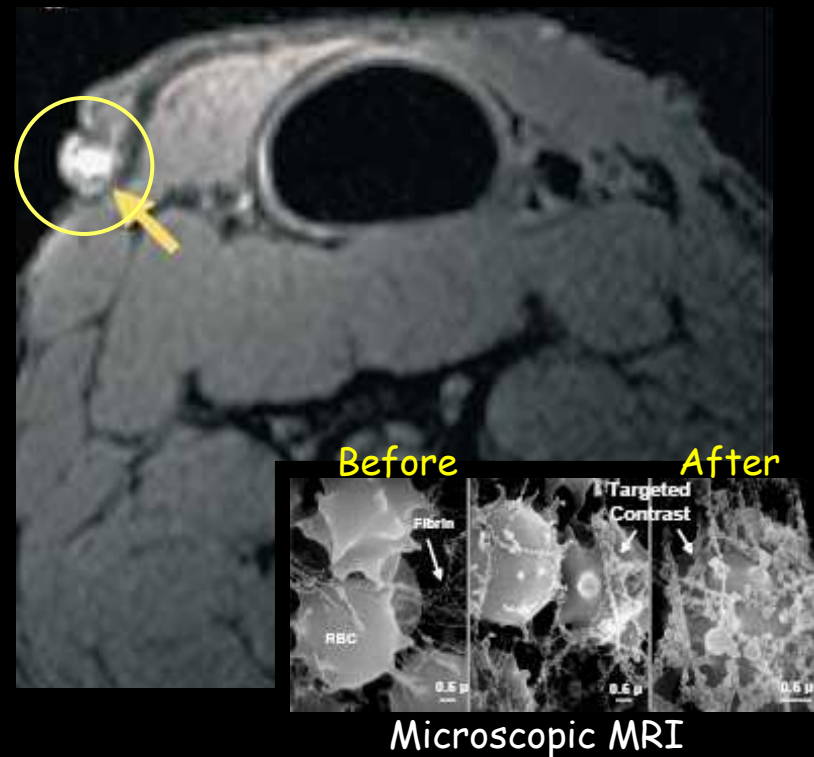
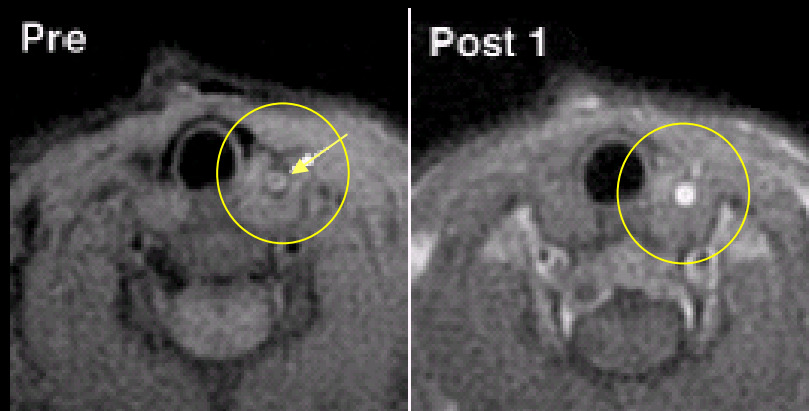


Lipids are mixed with the nanoparticles in an apolar solvent. The mixed film obtained is hydrated. Thereafter, the nanoparticle-containing micelles and empty micelles are separated by centrifugation

The targeting with fibrin-specific micelles containing paramagnetic nanoparticles visualizes thrombus in the external jugular vein

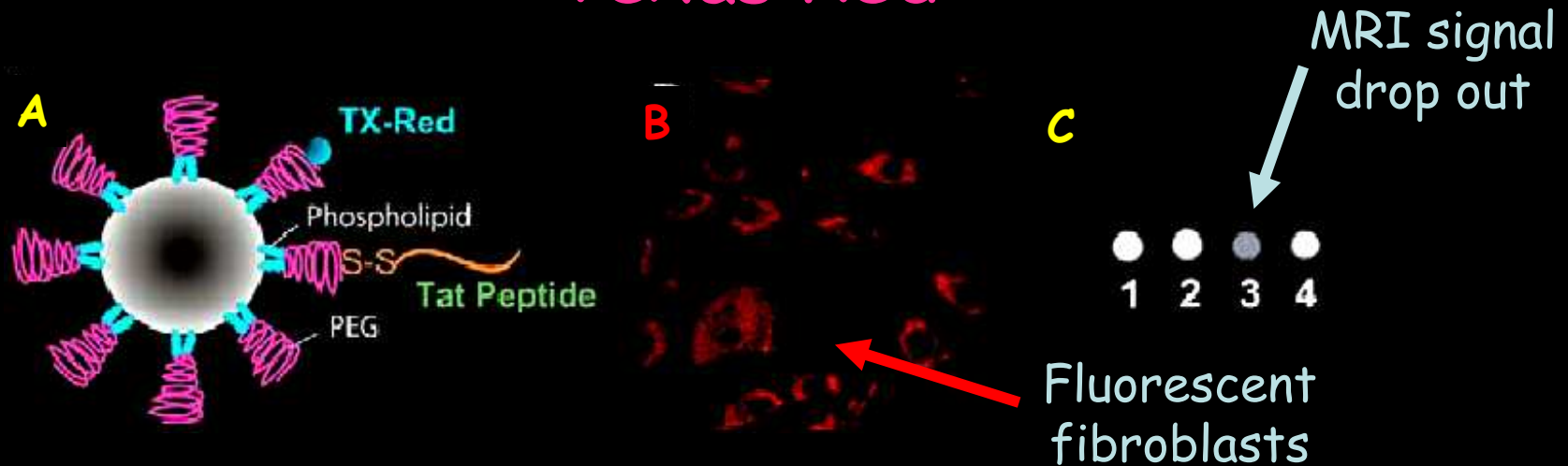
Fibrin plays the role of anti thrombic antigen

There exists a neat $T1_w$ contrast increase where paramagnetic nanoparticles conjugated to anti-fibrin antibody fragments accumulate (yellow arrows and circles).



FLACKE S, et al., Circulation, 2001 ; 104(11) : 1280-1285.

Micelle-encapsulated SPIO conjugated with Tat peptide and the fluorescent label Texas Red

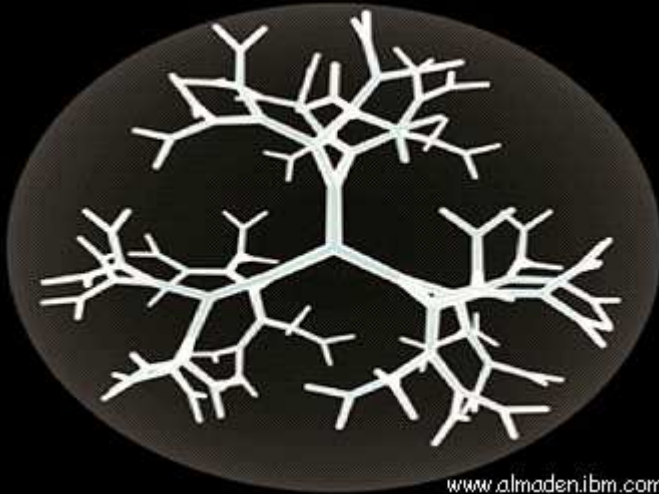


(A) Schematic of a micelle-encapsulated SPIO conjugated with Tat peptide and the fluorescent label Texas Red (TX-Red) for cellular delivery and combined optical imaging and MRI.

(B) Fluorescent images of Tat-linked, TX-Red-labeled SPIOs in human dermal fibroblast (HDF) cells. Images were obtained using a Zeiss confocal microscope with excitation at 543 nm and emission detection at 560 nm.

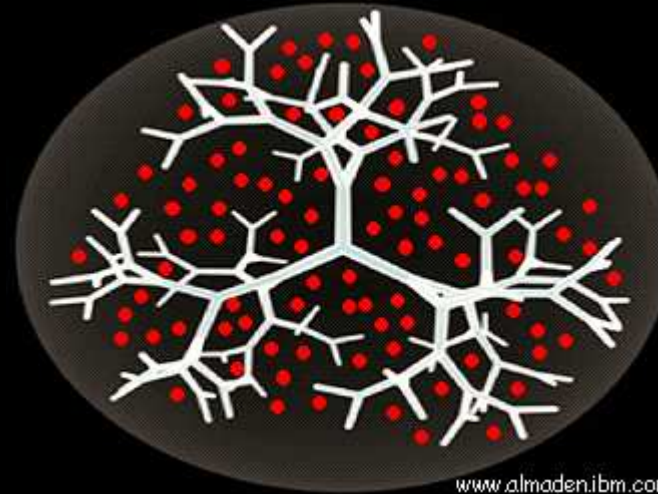
(C) MRI images of four different samples: (1) culture media only, (2) cells without SPIOs, (3) cells with SPIOs, (4) culture media only. Images were obtained using a 3 T Siemens TRIO MRI machine.

Over concentration of magnetic nano particles in dendrimers



www.almaden.ibm.com

"Virgin" dendrimer



www.almaden.ibm.com

Gd³⁺ or MION Magnetodendrimer

A dendrimer component is a polymeric, 3D tree-like structure

It contains a great number of 3D voids acting as pockets carrying numerous particles of contrast agent (Gd³⁺ or super-paramagnetic nanoparticles as MION).

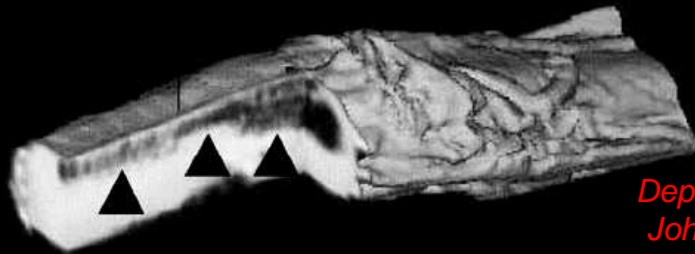
Magnetodendrimers allow efficient labeling of mammalian cells, including human neural stem cells and mesenchymal stem cells.

Their use in MRI allows growth tracking of new neural pathways from the stem cell transplant.

Nanotechnology and Medicine, Nanopedia, the web course of nanotechnology
<http://nanopedia.case.edu/NWPrint.php?page=nw.ppm2.med3>

Application of magnetodendrimers as cellular markers after transplantation

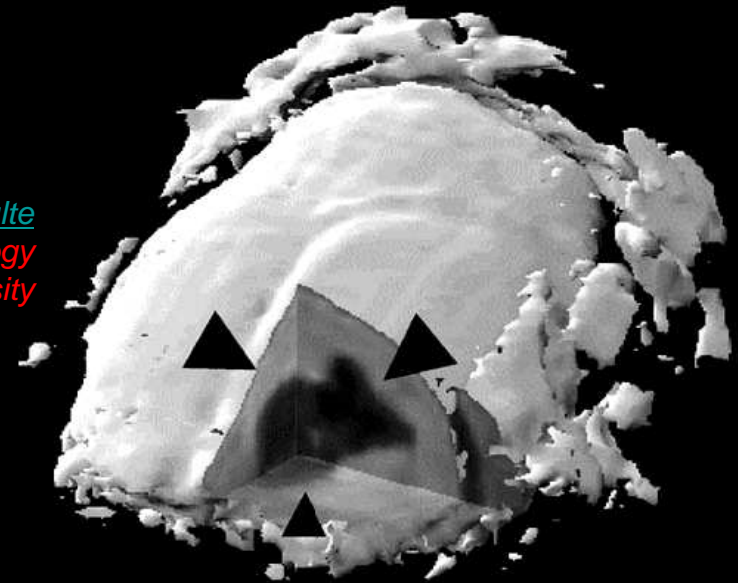
Stem cells containing magnetic nano particles in dendrimers were transplanted in dysmyelinated rat spinal cord



[Jeff Bulte](#)
Department of Radiology
John Hopkins University

At 10 days following transplantation, 3D *ex vivo* MR image shows the migration of labeled cells along the dorsal column away from the injection site.

There exists an excellent concordance between MRI and immunohistochemical coloration of new formed neural myelin



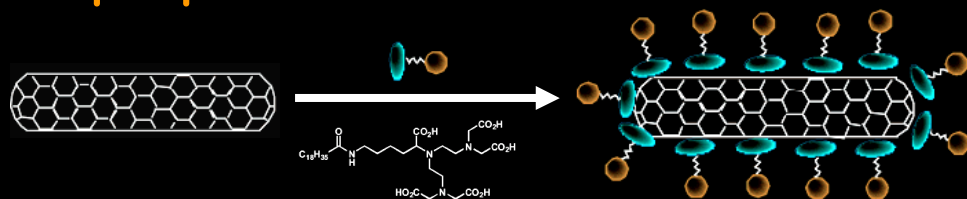
At 6 weeks following transplantation, 3D *in vivo* MR image shows the migration of labeled cells into the parenchyma away from the ventricle

JWM BULTE, Nature Biotech, 2001

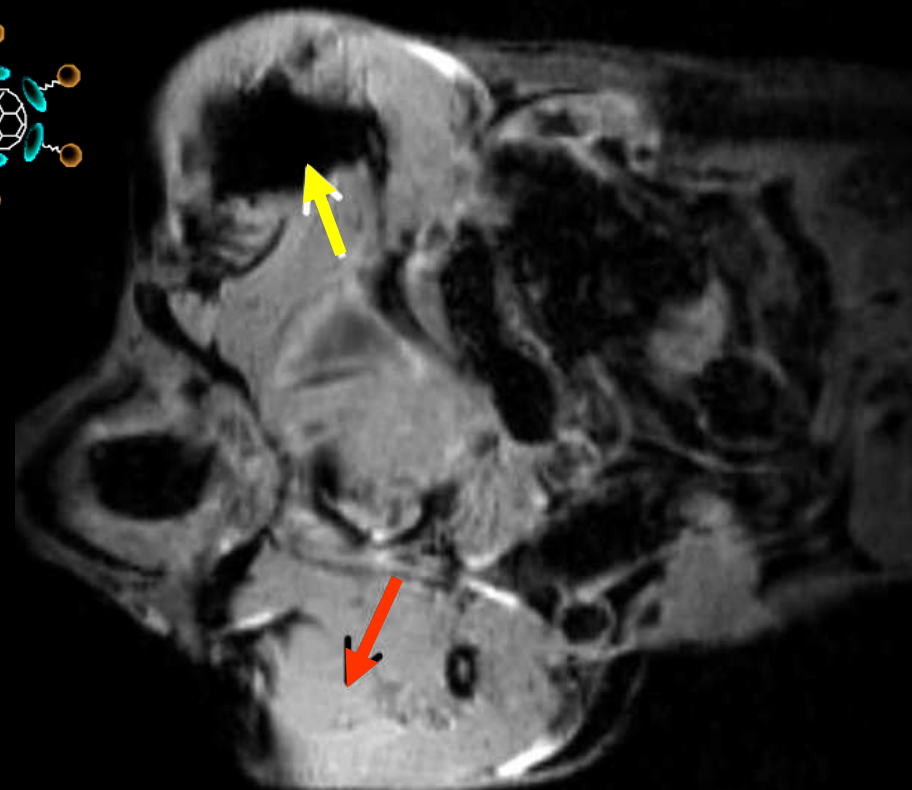
JWM BULTE, Journal of Magnetism and Magnetic Materials, 289 (2005) 423-427

Amplification and targeting with carbon nanotubes loaded with hydrated Gd^{3+} ions

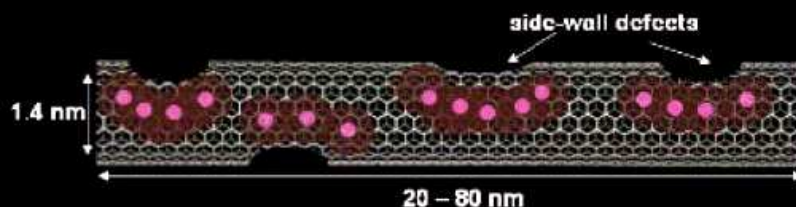
Carbon nanotubes can be noncovalently functionalized by amphiphilic Gd^{3+} chelates.



Coronal in vivo MR image of the muscle of a mouse legs
... after Gd^{3+} multiwalled carbon nanotubes injection
... and lipid injection



Here is another way to load carbon nanotubes with Gd^{3+}



C RICHARD, ET al., Nano Lett. 2008, Vol. 8, No. 1: 232-236

B. SITHARAMAN, et al., Chem. Commun., 2005, 3915-3917

Modifying images by activable contrasts

- smart or reporter agents
- Magnetic relaxation switch of CLIO
- Magnetic relaxation amplification
- Reporter gene imaging

Smart contrast agents

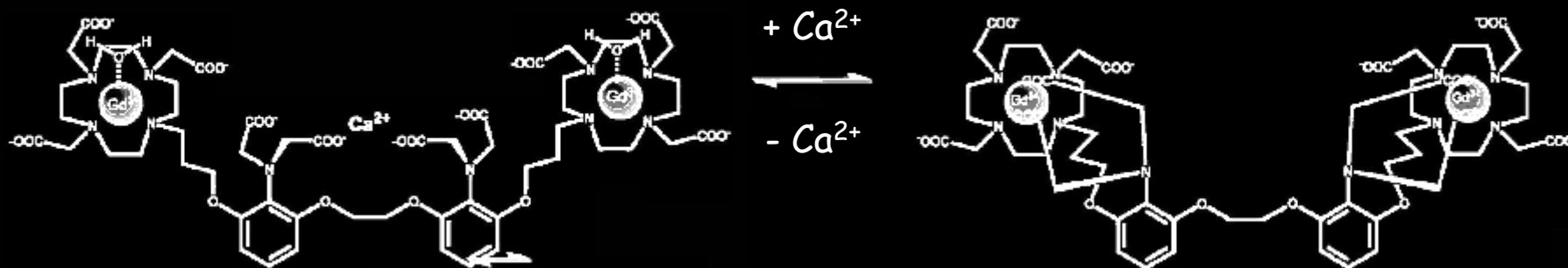
Smart contrast agents are activable agents that undergo a large change in relaxivity upon activation: one state is *off* and corresponds to low contrast enhancement, while the other state, the *on* state, corresponds to high contrast enhancement.

The activatable agent can be *switched* from one state to the other by the occurrence of a metabolic or physiological event.

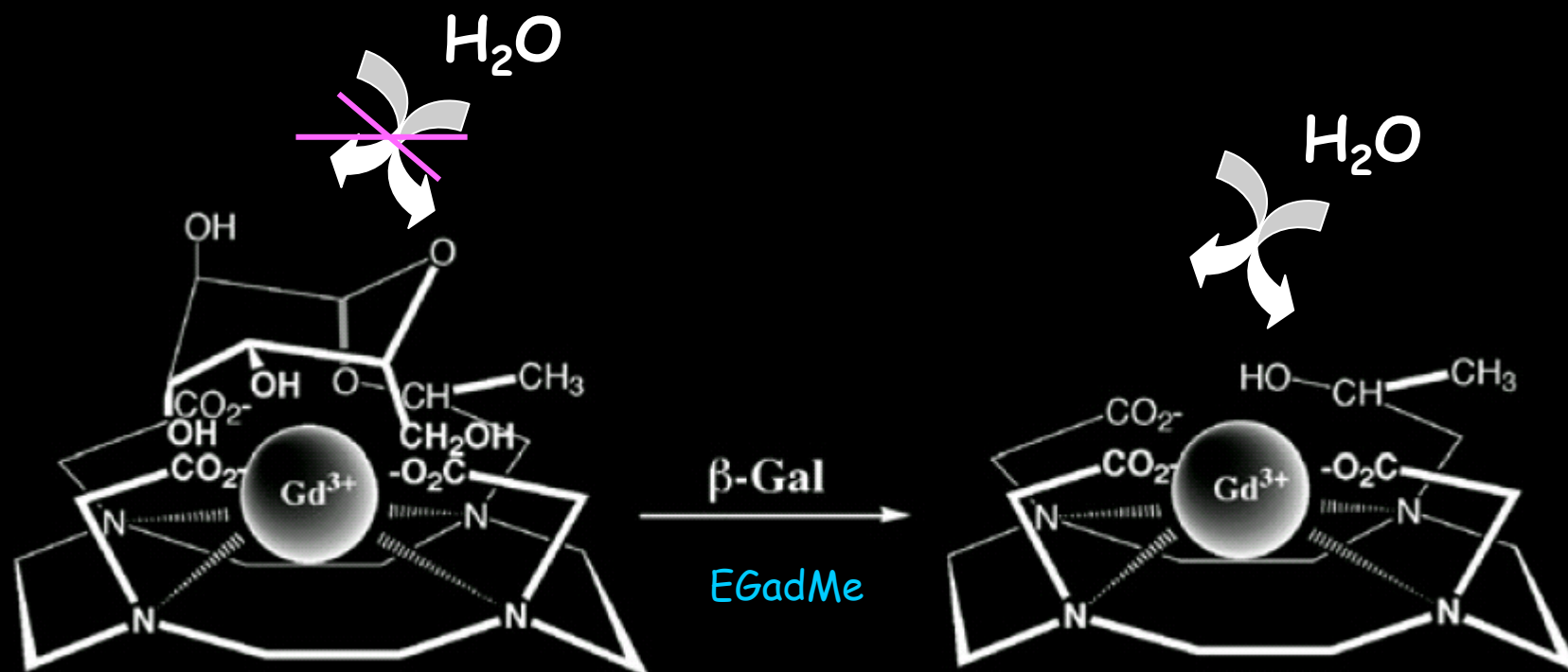
With Gd^{3+} agents, contrast enhancement is generally linked to a decrease in T1 but may follow a chemical exchange saturation transfer (CEST) event as the *switch*.

For iron oxide agents, contrast enhancement is due to an enhanced anisotropy that leads to a dramatic decrease in T2.

Examples of a "smart" MRI probes



DZIK-JURASZ, The British Journal of Radiology, 76 (2003), 598-5109



AY LOUIE et al., Nature biotechnology, March 2000, Volume 18 No 3 : 321-25

EGadMe - MRI detection of β -galactosidase mRNA expression in living *X. laevis* embryos



EGadMe has been used as a MR functional reporter agent for displaying *in vivo* β -galactosidase activity



Brighter images of *Xenopus* embryos injected with β -gal mRNA and EGadMe (top) compared with EGadMe alone (bottom)

Fluorochromes-labeled smart probe, activated by cathepsin-B

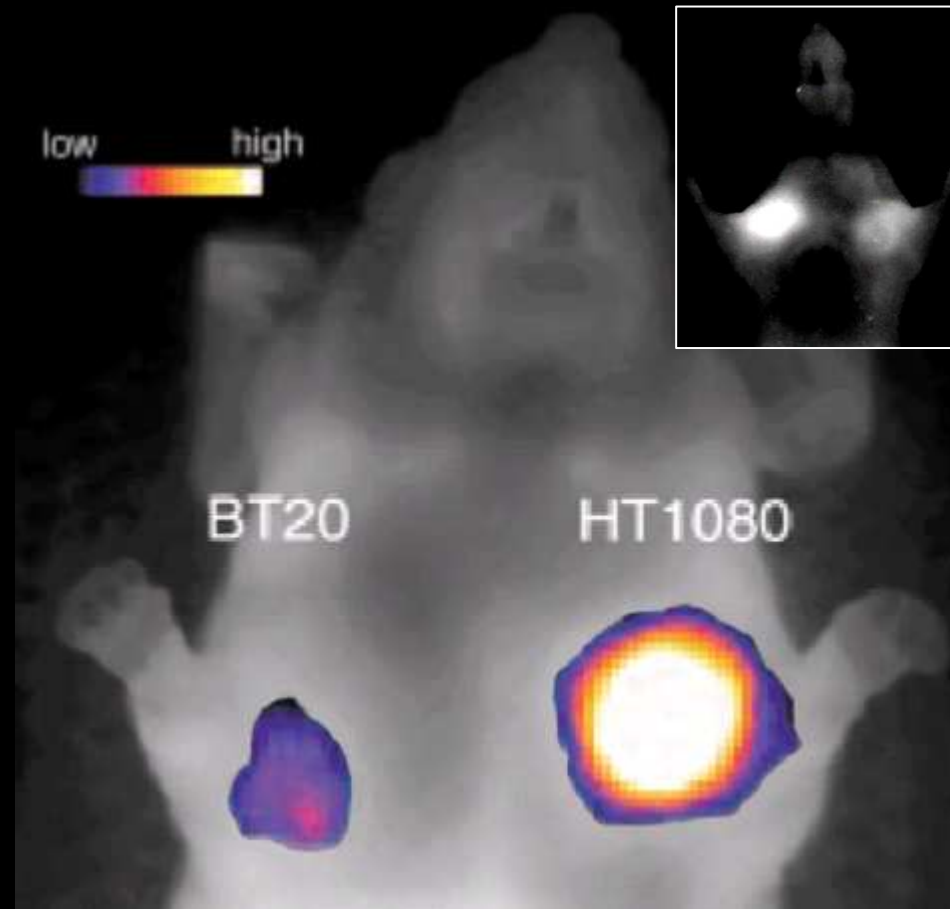


Image courtesy of Ralph Weissleder, CMIR

Color-encoded near-infrared fluorescence image of a mouse implanted with two different human breast tumors differing in tissue invasiveness.

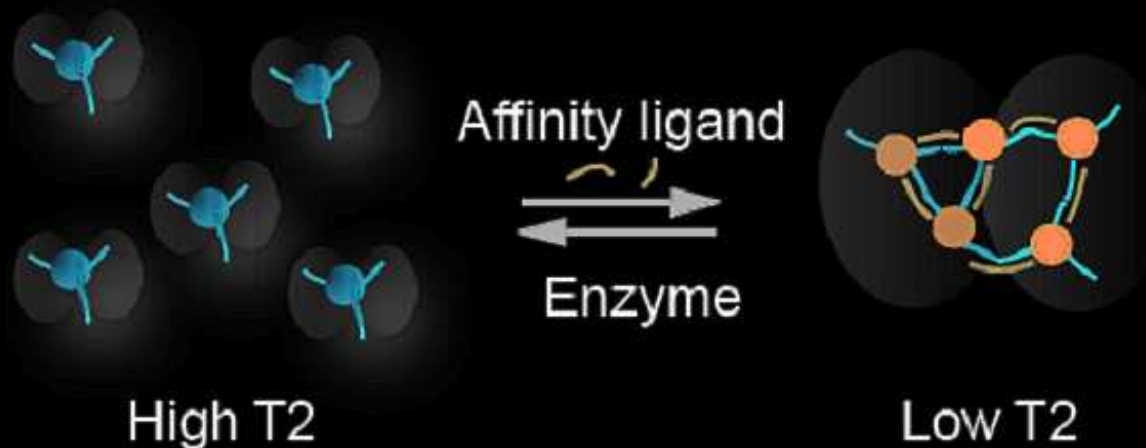
The mouse was injected with a fluorochromes-labeled smart probe, activated by cathepsin-B.

The agent is more activated in the more invasive right tumor (where is more cathepsin-B).

Magnetic relaxation switch of covalently coupled SPIO to biomolecules

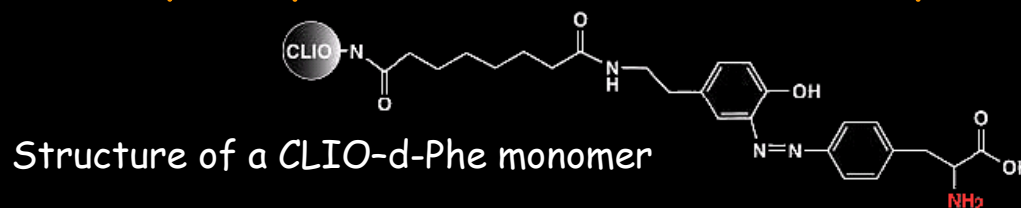
When (U)SPIO are covalently coupled to oligo-nucleotids, nucleic acids, small molecules, peptides, receptors ligands, proteins, antibodies, ..., they form CLIO (Cross Linked Iron Oxides), interacting with molecular targets (DNA, small molecules, proteins, enzymes, ...).

The cooperative auto aggregation of CLIO at the target level greatly increases their relaxing power by a local over concentration and a partial immobilization, allowing to visualize the aggregation site by the T2* hyposignal it implies

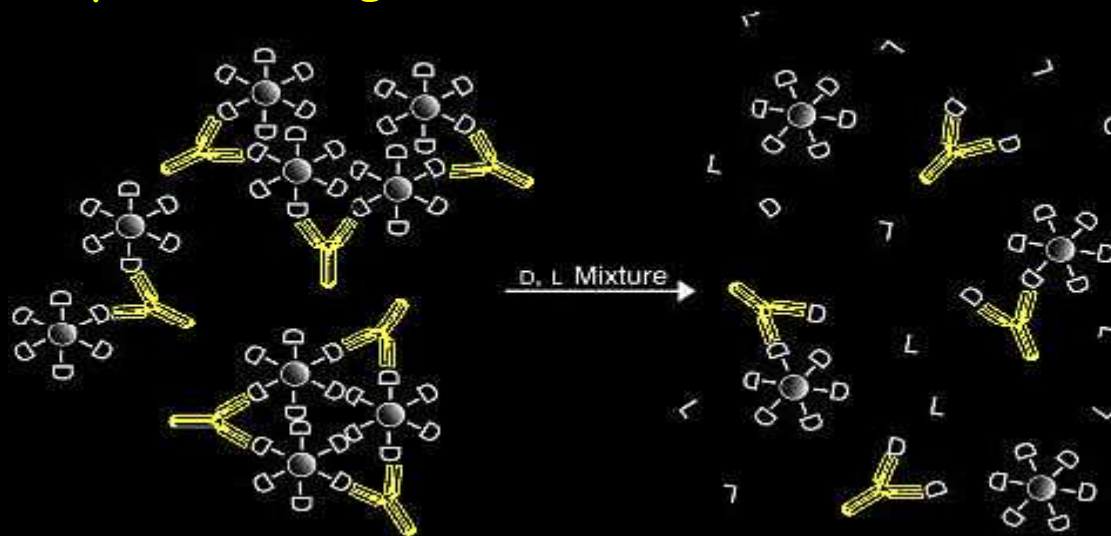


MR switch detection of L-Phenylalanine

In this example, a **CLIO**, made of an **SPIO** core coated with an **aminated dextran**, is covalently coupled to a derivative of d-phenylalanine (d-Phe)



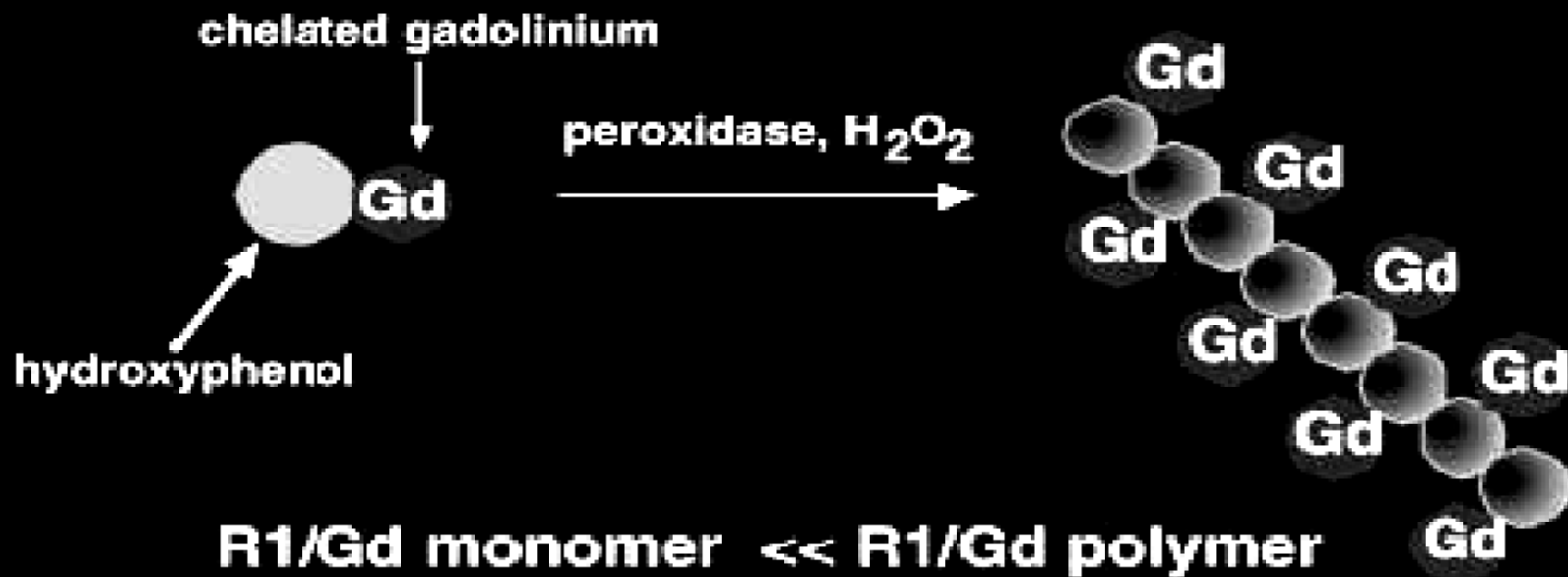
Addition of anti d-Amino Acids Antibody leads to monomers aggregation. The T_2^* relaxivity is thus high because of concentration & immobilization



When l-Phe is present, CLIO-d-Phe/anti d-AA aggregates disrupt, inducing a T_2^* relaxivity decrease leading to a signal increase by MR switch

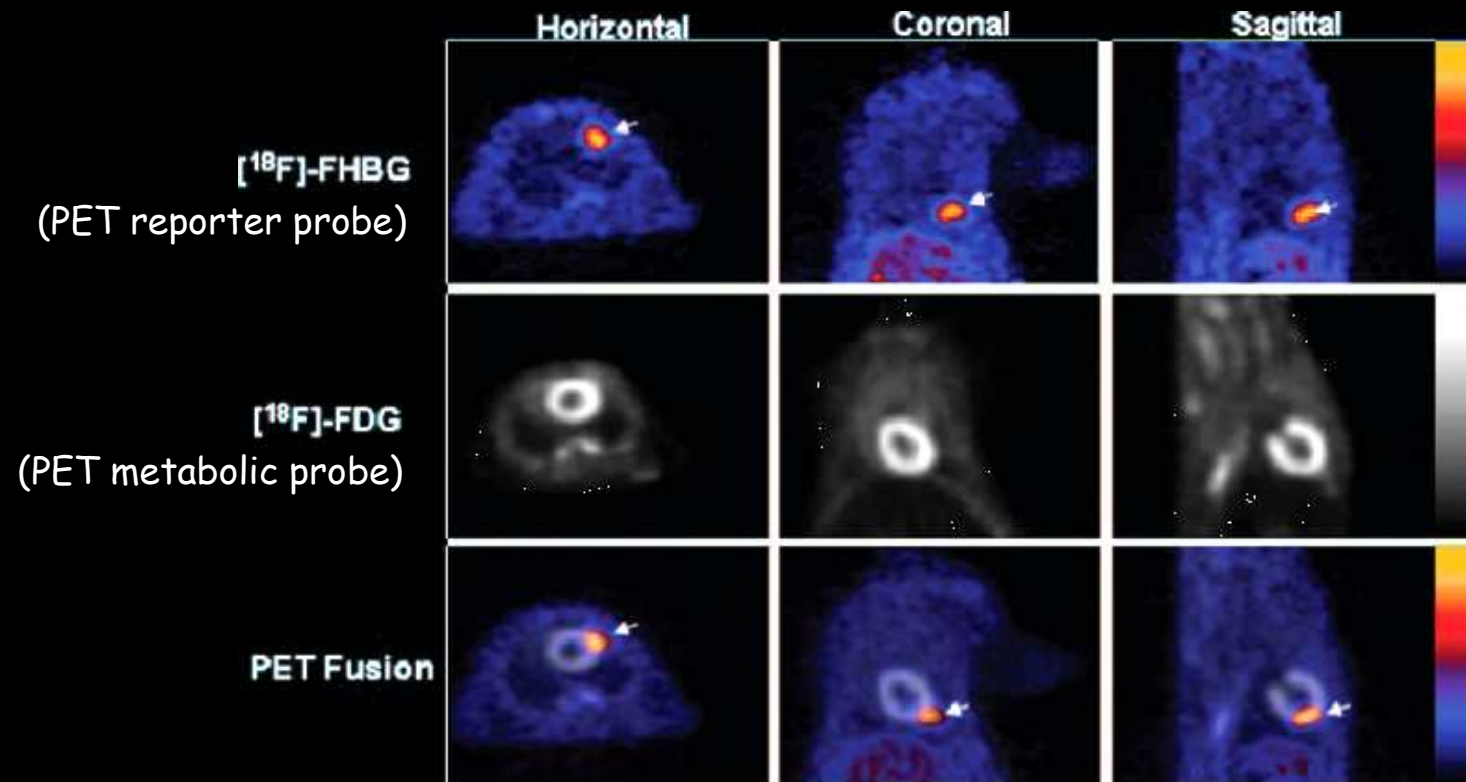
Magnetic relaxation amplification: Enzymatic activity by MRamp

Activation of hydroxyphenol by peroxidase in the presence of H_2O_2 results in spontaneous condensation and polymerization of chelated gadolinium and an hypersignal in T_{1w} MRI.



Reporter probe imaging

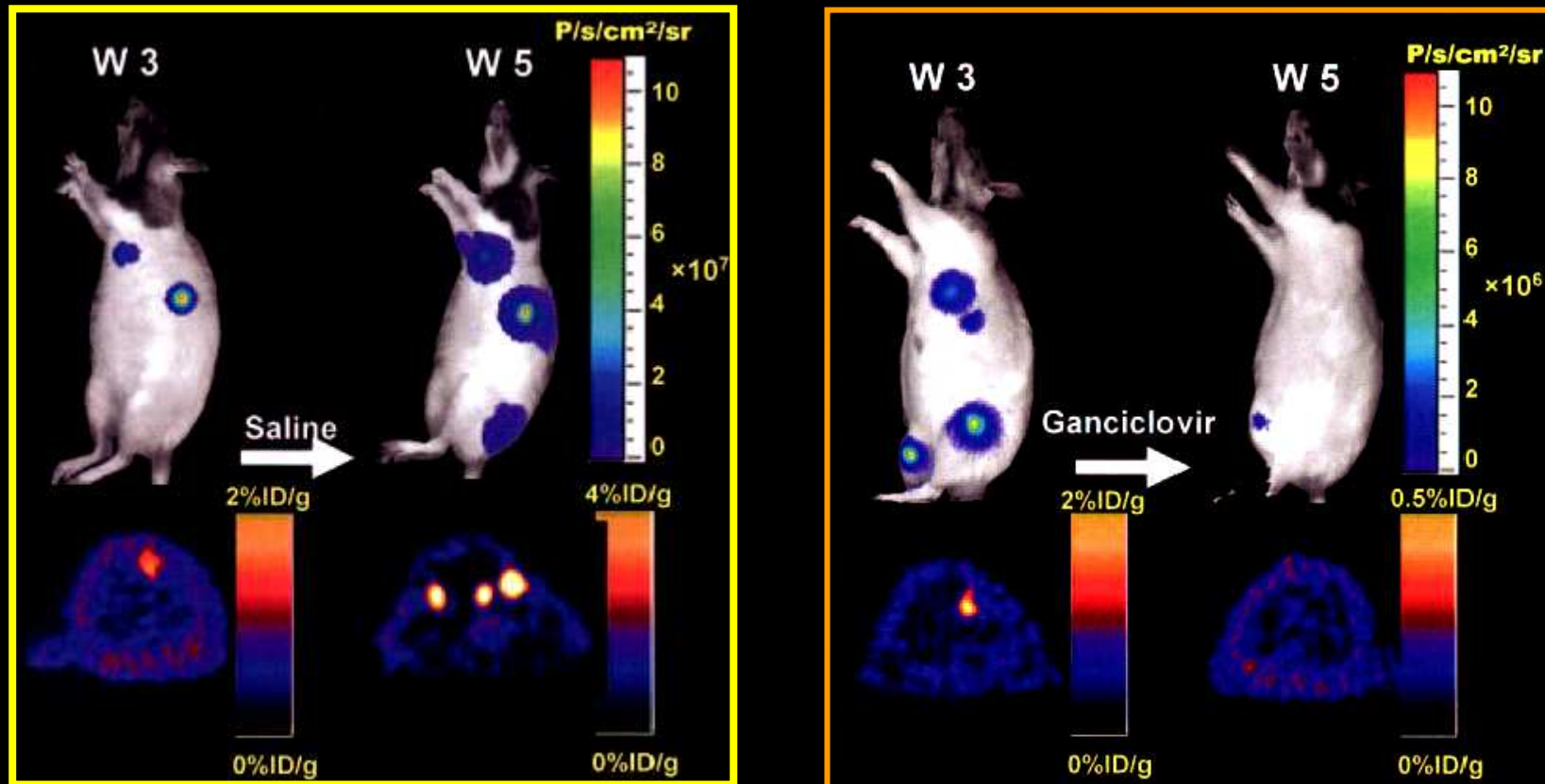
To define the location of transplanted Embryonic Stem cells in the myocardium, cells were stably transduced with a lentiviral vector carrying a novel triple-fusion (TF) reporter gene that consists of firefly luciferase, monomeric red fluorescence protein, and truncated thymidine kinase (fluc-mrfp-ttk).



Two weeks after cell transplantation, animals underwent [¹⁸F]- FHBG reporter probe imaging (top row) followed by [¹⁸F]-FDG myocardial viability imaging (middle row).

Embryonic Stem Cell-Derived Teratoma Formation Can Be Selectively Ablated by Ganciclovir Therapy

Ablation of teratoma formation with the PET reporter gene *ttk* (truncated thymidine kinase) as both a reporter and a suicide gene



Treatment of control animals with saline resulted in multiple teratoma formation by week 5. In contrast, study animals treated with ganciclovir for 2 weeks showed abrogation of both bioluminescence and PET imaging signals

Many thanks to ...

M 45 (Pleiades)

M DENAIN, CEA

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G HÉRIGAULT, Philips Medical Systems,

W KLUNK and C MATHIS ,

ME PHELPS,

... and all researchers whose work made this presentation possible

And thanks to all of you for kind listening